

Package ‘clintools’

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Type Package

Title Tools for Clinical Research

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Description Every research team have their own script for data management, statistics and most importantly hemodynamic indices. The purpose is to standardize scripts utilized in clinical research. The hemodynamic indices can be used in a long-format dataframe, and add both periods of interest (trigger-periods), and delete artifacts with deleter-files. Transfer function analysis (Claassen et al. (2016) <[doi:10.1177/0271678X15626425](https://doi.org/10.1177/0271678X15626425)>) and Mx (Czosnyka et al. (1996) <[doi:10.1161/01.str.27.10.1829](https://doi.org/10.1161/01.str.27.10.1829)>) can be calculated using this package.

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URL <https://github.com/lilleoel/clintools>

BugReports <https://github.com/lilleoel/clintools/issues>

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clinmon	<i>Hemodynamic Indices Calculated From Clinical Monitoring (clinmon)</i>
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Description

clinmon() uses a *continuous* recording and returns a dataframe with hemodynamic indices for every period, epoch or block depending on the input. Calculates COest, CPPopt, CVRi, Dx, Mx, PI, PRx, PWA, RI, and Sx (see *Hemodynamic indices*).

Usage

```
clinmon(df, variables,
        trigger = NULL, deleter = NULL,
        blocksize = 3, epochsize = 20,
        overlapping = FALSE, freq = 1000,
        blockmin = 0.5, epochmin = 0.5,
        output = "period", fast = FALSE)
```

Arguments

df	Raw <i>continuous</i> recording with all numeric data and first column has to be time in seconds. (dataframe)
variables	Defining the type and order of the recorded variables as a list. Middle cerebral artery blood velocity ('mcav'), Arterial blood pressure ('abp'), cerebral perfusion pressure ('cpp'), intracranial pressure ('icp'), and heart rate ('hr') is currently supported. <i>It is necessary that time is the first row.</i> (list)

trigger	Trigger with two columns: first is start, and second is end of periods to be analyzed. Every row corresponds to a period. Default is NULL, which results in analysis of the full dataframe. (dataframe)
deleter	Deleter with two columns: first is start and second is end of period with artefacts, which need to be deleted. Every row is a period with artefacts. Default is NULL. (dataframe)
blocksize	Length of a block, in seconds. Default is 3. (numeric)
epochsize	Size of epochs in number of blocks. Default is 20. (numeric)
overlapping	The number of block which should overlap when calculating correlation based indices, and remain blank if overlapping calculations should not be utilized. Default is FALSE. (numeric)
freq	Frequency of recorded data, in Hz. Default is 1000. (numeric)
blockmin	Minimum measurements required to create a block in ratio. Default is 0.5 corresponding to 50%. If the block holds less than the defined ratio the block will be omitted. (numeric)
epochmin	Minimum number of blocks required to create an epoch in ratio. Default is 0.5 corresponding to 50%. If the epoch holds less than the defined ration the epoch will be omitted. (numeric)
output	Select what each row should represent in the output. Correlation based indices are not presented when selecting blocks for every row. Currently 'block', 'epoch', 'period' or 'cpopt' is supported. Default is 'period'. (string)
fast	Select if you want the data to aggregated before analysis resulting in a faster, but perhaps more imprecise run, in Hz. Default is FALSE. (numeric)

Details

Using a *continuous* raw recording, `clinmon()` calculates hemodynamic indices for every period, epoch or block depending on the chosen output.

View(data)

```

      time  abp  mcav
      7.00   78   45
      7.01   78   46
      ...   ...   ...
    301.82   82   70
    301.83   81   69

```

To calculate the indices insert the data and select the relevant variables.

```
clinmon(df=data, variables=c("abp", "mcav"))
```

See **Value** for output description.

Value

Returns a dataframe with the results, with either every blocks, epochs or periods as rows, depending on the chosen output.

The columns of the output are:

- period - The period number corresponding to the row-number in the trigger file.
- epoch - The epoch number, or if period is chosen as output it reflects the number of epochs in the period.
- block - The block number, or if period or epoch is chosen as output it reflects the number of blocks in the period or epoch.
- time_min - The minimum time value or the period, epoch or block.
- time_max - The maximum time value or the period, epoch or block.
- missing_percent - The percentage of missing data in the period, epoch or block.
- XX_mean - The mean value of each variable for the period, epoch or block.
- XX_min - The minimum value of each variable for the period, epoch or block.
- XX_max - The maximum value of each variable for the period, epoch or block.
- YY - The indices in each column.

Hemodynamic indices**COest | Estimated cardiac output:**

Required variables: abp, hr; *Required output:* -.

Estimated cardiac output (COest) is calculated by utilizing the method described by Koenig et al. [1]:

$$CO_{est} = PP / (SBP + DBP) * HR$$

PP: Pulse pressure; SBP: systolic blood pressure; DBP: diastolic blood pressure; HR: heart rate.

CPPopt | Optimal cerebral perfusion pressure:

Required variables: abp, icp; *Required output:* period.

Optimal cerebral perfusion pressure (CPPopt) is calculated utilizing the method described by Steiner et al. [2]. The CPPopt return NA if CPPopt is the maximum or minimum CPP investigated. CPPopt is recommended to only be calculated after 'several hours' of recording:

$$CPP_{opt} = The5mmHgCPPIntervalWithLowestMeanPRx$$

CPP: cerebral perfusion pressure; PRx: Pressure reactivity index.

CVRi | Cardiovascular resistance index:

Required variables: abp, mcav; *Required output:* -.

Cardiovascular resistance index (CVRi) is calculated utilizing the method described by Fan et al. [3]:

$$CVRi = meanABP / meanMCAv$$

ABP: arterial blood pressure; MCAv: middle cerebral artery blood velocity.

Dx | Diastolic flow index:

Required variables: cpp/abp, mcav; *Required output:* epoch, period.

Diastolic flow index (Dx) is calculated utilizing the method described by Reinhard et al. [4]:

$$Dxc = cor(meanCPP/minMCAv)$$

$$Dxa = cor(meanABP/minMCAv)$$

cor: correlation coefficient; CPP: cerebral perfusion pressure; ABP: arterial blood pressure; MCAv: middle cerebral artery blood velocity.

Mx | Mean flow index:

Required variables: cpp/abp, mcav; *Required output:* epoch, period.

Mean flow index (Mx) is calculated utilizing the method described by Czosnyka et al. [5]:

$$Mxc = cor(meanCPP/meanMCAv)$$

$$Mxa = cor(meanABP/meanMCAv)$$

cor: correlation coefficient; CPP: cerebral perfusion pressure; ABP: arterial blood pressure; MCAv: middle cerebral artery blood velocity.

PI | Gosling index of pulsatility:

Required variables: mcav; *Required output:* -.

Gosling index of pulsatility (PI) is calculated utilizing the method described by Michel et al. [6]:

$$PI = (systolicMCAv - diastolicMCAv)/meanMCAv$$

MCAv: middle cerebral artery blood velocity.

PRx | Pressure reactivity index:

Required variables: abp, icp; *Required output:* epoch, period.

Pressure reactivity index (PRx) is calculated utilizing the method described by Czosnyka et al. [7]:

$$PRx = cor(meanABP/meanICP)$$

cor: correlation coefficient; CPP: cerebral perfusion pressure; ICP: intracranial pressure.

PWA | Pulse wave amplitude:

Required variables: cpp/icp/abp/mcav; *Required output:* -.

Pulse wave amplitude (PWA) is calculated utilizing the method described by Norager et al. [8]:

$$PWA = systolic - diastolic$$

RI | Pourcelots resistive (resistance) index:

Required variables: mcav; *Required output:* -.

Pourcelots resistive (resistance) index (RI) is calculated utilizing the method described by Forster et al. [9]:

$$RI = (systolicMCAv - diastolicMCAv)/systolicMCAv$$

MCAv: middle cerebral artery blood velocity.

Sx | Systolic flow index:

Required variables: cpp/abp, mcav; *Required output:* epoch, period.

Systolic flow index (Sx) is calculated utilizing the method described by Czosnyka et al. [5]:

$$Sxc = cor(meanCPP/systolicMCAv)$$

$$Sxa = cor(meanABP/systolicMCAv)$$

cor: correlation coefficient; CPP: cerebral perfusion pressure; ABP: arterial blood pressure; MCAv: middle cerebral artery blood velocity.

References

1. Koenig et al. (2015) Biomed Sci Instrum. 2015;51:85-90. ([PubMed](#))
2. Steiner et al. (2002) Crit Care Med. 2002 Apr;30(4):733-8. ([PubMed](#))
3. Fan et al. (2018) Front Physiol. 2018 Jul 16;9:869. ([PubMed](#))
4. Reinhard et al. (2003) Stroke. 2003 Sep;34(9):2138-44. ([PubMed](#))
5. Czosnyka et al. (1996) Stroke. 1996 Oct;27(10):1829-34. ([PubMed](#))
6. Michel et al. (1998) Ultrasound Med Biol. 1998 May;24(4):597-9. ([PubMed](#))
7. Czosnyka et al. (1997) Neurosurgery. 1997 Jul;41(1):11-7; discussion 17-9. ([PubMed](#))
8. Norager et al. (2020) Acta Neurochir (Wien). 2020 Dec;162(12):2983-2989. ([PubMed](#))
9. Forster et al. (2017) J Paediatr Child Health. 2018 Jan;54(1):61-68. ([PubMed](#))

Examples

```
data(testdata)
clinmon(df.data10, variables=c('abp', 'mcav', 'hr'), freq=10)
```

df.data1000

Test-data - 1000 Hz

Description

Recording with four columns: time (t), non-invasive arterial blood pressure (abp), middle cerebral artery velocity measured using transcranial Doppler (mcav), and heart rate (hr).

Usage

```
data(testdata)
```

Format

An object of class "dataframe"; an example of the usage in [clinmon](#)-function.

References

Olsen MH et al. (Unpublished data, 2020) ([GitHub](#))

Examples

```
data(testdata)
variables <- c("abp", "mcav", "hr")
clinmon(df.data1000, variables, fast=50)
```

df.deleter

Test-deleter

Description

Deleter dataframe with two columns: start (start) and end (end) of the deleter-period.

Usage

```
data(testdata)
```

Format

An object of class "dataframe"; an example of the usage in [clinmon](#)-function.

References

Olsen MH et al. (Unpublished data, 2020) ([GitHub](#))

Examples

```
data(testdata)
variables <- c("abp", "mcav", "hr")
clinmon(df.data1000, variables, deleter=df.deleter, fast=50)
```

dilations

Assess dilations from PLR3000-output.

Description

dilations() is a function which converts longformat recording of pupillary size and uses markers to generate a dataframe, plot, and markdown output to inspect the results.

Usage

```
dilations(pupils, markers,
  remove_markers = NULL, add_markers = NULL,
  not_assess = NULL, artefacts_static = c(0.55,9.95),
  artefacts_dynamic = c(`1` = 1.5, `0.66` = 1, `0.33` = 0.5),
  time_assess = c(`1` = 10, `3` = 5),
  sig.level = 0.05, min_change = NULL,
  resting_delay = c(`3` = 0))
```

Arguments

pupils	recording of pupillary function. long format dataframe with at least three columns: record_id, time, and size.
markers	time of markers. long format dataframe with at least two columns: record_id and time.
remove_markers	markers which should be removed. long format dataframe with at least two columns: record_id and time. The time column need one decimal.
add_markers	markers which should be added. long format dataframe with at least two columns: record_id and time. The time column need one decimal.
not_assess	a list of record ids which should no be assessed.
artefacts_static	a list of the limits of the artefacts. The first number in the list is the minimum size to be assessed and the second is the maximum size to be assessed
artefacts_dynamic	a named list where max change in millimeter within the duration (name in list) is removed. Will use the first 1 second of the recording to create a baseline, thus susceptible to artefacts in the start of the recording.
time_assess	This named list define the number of seconds which should be used in the assessment of dilations. The name is the number of periods-of-interest and the value is the seconds.
sig.level	This is the significance level to be used when comparing the size of the period-of-interest. The significance level corresponds to the Wilcox.test used.
min_change	This is the minimum size of mm which needs to change before a dilation can be identified. Default is no minimum requirement.
resting_delay	This can be used if the subsequent resting period to compare should be delayed, i.e. if we should wait 5 second for those investigations with three periods of interest create a named list with periods of interest as names and seconds to delay as input.

Value

Returns a nested list one dataframe of the results (`$dilations`), plot (`$plot$id[record id]`), and a markdown output (`$plot$markdown$id[record id]`). The dilations dataframe include the following columns: Record ID (`record_id`); Patient ID (`pt_id`); Date (`date`); pupil side (`side`); start of the period (`min`); end of the period (`max`); length of period (`rec_length`); number of measurements (`n`); median size (`median`); P value when comparing with the previous period (`p_before`); P value when

comparing with the following period (p_after); and if dilation is identified (dilation, 1 is successful dilation and 0 is no dilation).

Examples

```
## Not run:
recordings <- PLR3000("C:/PLR3000/R_20200105_205901.xls")
dilations <- dilations(recordings$pupils,recordings$markers)

# The dataframe of the results
dilations$dilations

# The plot of one of the recordings
dilations$plot$id833

# The markdown output of one of the recordings
dilations$markdown$id833

## End(Not run)
```

iscus

ISCUSFlex-values to dataframe (iscus)

Description

iscus() is a function which converts XML files extracted from the Microdialysis-apparatur of ISCUSFlex apparatus to a dataframe.

Usage

```
iscus(filename)
```

Arguments

filename path to the XML-file with the measurements

Value

Returns a dataframe with the measurements.

Examples

```
## Not run:
iscus("C:/ISCUSfiles/7888e844-1c7a-40af-a3f2-3bb27a8dd9e5.xml")

## End(Not run)
```

ortable	<i>Logistic regression table with Odds ratio (ortable)</i>
---------	--

Description

ortable() is a small function which utilises the output from the glm-function to print a dataframe with odds ratio, confidence limits, and p-values.

Usage

```
ortable(x, d, d_p, intercept, simple)
```

Arguments

x	Utilises the output from a glm-function. (glm-output)
d	Refers to the number of digits for odds ratio and confidence intervals. Default is 2. (numeric)
d_p	Refers to the number of digits for odds ratio and confidence intervals. Default is 3. (numeric)
intercept	The intercept is presented in the table if TRUE. Default is FALSE. (boolean)
simple	Odds ratio and confidence intervals are merged into one column if TRUE. Default is TRUE. (boolean)

Value

Returns a dataframe with with odds ratio, confidence limits, and p-values.

Examples

```
df <- data.frame(outcome=sample(0:1, 100,replace=TRUE),
  var=sample(0:100,100,replace=TRUE))
ortable(glm(outcome ~ ., data=df))
```

PLR3000	<i>NeuroOpticsTM PLR-3000 pupillometer file to dataframe (PLR3000)</i>
---------	--

Description

PLR3000() is a function which converts the XLS file imported from the eurOpticsTM PLR-3000 pupillometer to a nested list with two dataframes.

Usage

```
PLR3000(filename = NULL, df = NULL)
```

Arguments

filename path to the XLS-file with the measurements
df the dataframe can also be used for the function if data is already imported.

Value

Returns a list with two dataframe, one with the measurements (pupils) and one with the markers (markers).

Examples

```
## Not run:
  PLR3000("C:/PLR3000/R_20200105_205901.xls")

## End(Not run)
```

rrGcomp	<i>Relative risk derived by G-computation (rrGcomp)</i>
---------	---

Description

rrGcomp() is a small function which generates population-level (marginal) relative risks derived by G-computation. For models with random effects mixed-effects generalized linear model with a logit link with adjustment for stratification variables will be used, while those without random effects a logistic regression will be used. The code is based on the method used in the paper by Dankiewicz et al. (2021) N Engl J Med. Jun 17;384(24):2283-2294. ([PubMed](#))

Usage

```
rrGcomp(df, outcome_col, group_col,
         fixed_strata = NULL, random_strata = NULL,
         nbrIter = 5000, conf_level = 0.95)
```

Arguments

df the individual participant dataframe
outcome_col column name for the outcome column
group_col column name for the group column
fixed_strata list of column names for the fixed effect stratification columns
random_strata list of column names for the random effect stratification columns
nbrIter number of iterations to be used in the G-computation. The original paper used 5000, which is also the default.
conf_level the confidence level to be reported.

Value

Returns a list with relative risk (rr), simulated rr (simRR), lower- and upper confidence level (simLCL/simUCL), and the p-value (p_val)

Examples

```
df <- sRCT(n_sites=3,n_pop=50)
rrGcomp(df,outcome_col="outcome",group_col="Var1",random_strata="site",nbrIter=10)
```

sRCT

*simulated Randomised Clinical Trial (sRCT)***Description**

sRCT() is a function which simulates a randomised clinical trial with a binary outcome and returns a dataframe. This version is validated to be used for analysis of interaction in a factorial design.

Usage

```
sRCT(all_sizes = NULL, n_pop = 1000,
n_sites = 10, design = c(2,2,2),
rrr = c(0.05,0.05,0), outcome_risk = 0.492,
interaction = c(`1-2` = 0.05, `1-2-3` = -0.05),
site_re = 0.05)
```

Arguments

all_sizes	Size of blocks in allocation table. If left empty the three lowest possible block sizes will be randomly assigned.
n_pop	Number of participants included in the trial.
n_sites	Number of sites
design	Number of sites as a list where each element corresponds to an intervention and the number in the element is the number of groups. So for a 2x2 factorial design c(2,2) should be used.
rrr	relative risk reduction for each intervention so for the abovementioned 2x2 factorial design with RRR of 0.05 and 0.10 we would use c(0.05, 0.10).
outcome_risk	The baseline risk (probability in absolute percentage) of the dichotomous primary outcome.
interaction	Interaction between interventions with a named list. If interaction exists between intervention 1 and 2 we would use 1-2 = 0.05.
site_re	The size of the random effect of site, default is 0.05.

Details

The sRCT function is continuously being developed to answer specific questions in simulation studies. sRCT will be updated and tested for each specific question. For each update the function will be validated for the current purpose and all previous purposes. sRCT is not validated for all simulation studies

Value

Returns a dataframe with an individual participant data frame.

Examples

```
sRCT()
```

testdata10	<i>Test-data - 10 Hz</i>
------------	--------------------------

Description

Recording with four columns: time (t), non-invasive arterial blood pressure (abp), middle cerebral artery velocity measured using transcranial Doppler (mcav), and heart rate (hr).

Usage

```
data(testdata)
```

Format

An object of class "dataframe"; an example of the usage in [clinmon](#)-function.

References

Olsen MH et al. (Unpublished data, 2020) ([GitHub](#))

Examples

```
data(testdata)
variables <- c("abp", "mcav", "hr")
clinmon(df.data10, variables, freq=10)
```

Description

TFA() calculates dynamic cerebral autoregulation through a transfer function analysis from a *continuous* recording. This function follows the recommendations from Claassen et al. [1] and mimicks the matlab script created by David Simpsons in 2015 ([Matlab TFA function](#)). TFA() also includes the possibility to analyse raw recordings with application of cyclic (beat-to-beat) average with the possibility of utilizing interpolation. (see **details**).

Usage

```
TFA(df, variables,
    trigger = NULL, deleter = NULL,
    freq = 1000, fast = 50, raw_data = FALSE,
    interpolation = 3, output = "table",
    vlf = c(0.02,0.07), lf = c(0.07,0.2),
    hf = c(0.2,0.5), detrend = FALSE,
    spectral_smoothing = 3,
    coherence2_thresholds = cbind(c(3:15),
    c(0.51,0.40,0.34,0.29,0.25,0.22,0.20,0.18,
    0.17,0.15,0.14,0.13,0.12)),
    apply_coherence2_threshold = TRUE,
    remove_negative_phase = TRUE,
    remove_negative_phase_f_cutoff = 0.1,
    normalize_ABP = FALSE,
    normalize_CBFV = FALSE,
    window_type = 'hanning',
    window_length = 102.4,
    overlap = 59.99,
    overlap_adjust = TRUE,
    na_as_mean = TRUE)
```

Arguments

df	Raw <i>continuous</i> recording with numeric data and first column has to be time in seconds. (dataframe)
variables	Definition of the type and order of recorded variables as a list. Middle cerebral artery blood velocity ('mcav') and arterial blood pressure ('abp') is currently supported. (list)
trigger	Trigger with two columns: first is start, and second is end of period to be analyzed. Every row is a period for analysis. Default is NULL, which results in analysis of the full dataframe. (dataframe)
deleter	Deleter with two columns: first is start and second is end of period with artefacts, which need to be deleted. Every row is a period with artefacts. Default is NULL. (dataframe)

freq	Frequency of recorded data, in Hz. Default is 1000. (numeric)
fast	Select if you want the data to aggregated resulting in a faster, but perhaps more imprecise run, in Hz. Default is 50 (numeric)
raw_data	Select TRUE if the data is raw and cyclic mean should be calculated. NB: this function have not been validated, why validated methods for calculating cyclic mean are preferred. Only 1 period can be analysed using raw_data. Default is FALSE (boolean)
interpolation	Select the number of beats which should be interpolated. Default is up to 3 beats and 0 results in no interpolation. (numeric)
output	Select what the output should be. 'table' results in a dataframe with values for the three frequencies defined by Claassen et al. [1]; 'long' results in a dataframe with the results in a long format; 'plot' results in a dataframe which can help plot gain, phase and coherence; 'plot-peak' results in a dataframe, which can be used to validate the cyclic average, and 'raw' results in a nested list with results primarily for debugging. Default is 'table'. (string)
vlf, lf, hf, detrend, spectral_smoothing, coherence2_thresholds	See TFA-parameters
apply_coherence2_threshold, remove_negative_phase	See TFA-parameters
remove_negative_phase_f_cutoff, normalize_ABP	See TFA-parameters
normalize_CBFV, window_type, window_length, overlap	See TFA-parameters
overlap_adjust, na_as_mean	See TFA-parameters

Details

Using a *continuous* raw recording, TFA() calculates dynamic cerebral autoregulation trough a transfer function analysis. This function utilizes the recommendations from Claassen et al [1] and mimicks the matlab script created by David Simpsons in 2015.

```
View(data)
```

```

      time  abp  mcav
      7.00   78   45
      7.01   78   46
      ...   ...   ...
    301.82   82   70
    301.83   81   69

```

To calculate the variables insert the data and select the relevant variables.

```
TFA(df=data, variables=c("abp", "mcav"))
```

See **Value** for output description.

Value

TFA() returns a dataframe depending on the output selected. 'table' results in a dataframe with values for the three frequencies defined by Claassen et al. [1]; 'long' results in a dataframe with the results in a long format; 'plot' results in a dataframe which can help plot gain, phase and coherence; 'plot-peak' results in a dataframe, which can be used to validate the cyclic average, and 'raw' results in a nested list with results primarily for debugging.

Some generic variables are listed below:

- abp_power - The blood pressure power measured in mmHg².
- cbfv_power - The cerebral blood flow velocity power measured in cm²*s⁻²
- coherence - Coherence.
- gain_not_normal - Not normalized gain measured in cm*s⁻¹*mmHg⁻¹.
- gain_normal - Normalized gain measured in %*mmHg⁻¹.
- phase - Phase measured in radians.

output = 'table':

Wide format output table with period, VLF, LF, and HF as columns, and the TFA-variables as rows.

period	variable	vlf	lf	hf
1	abp_power	6.25	1.56	0.21
1	cbfv_power	3.22	2.25	0.30
...
3	gain_normal	1.04	1.48	1.85
3	phase	53.0	25.4	9.38

output = 'long':

Long format output table which can be manipulated depending on the intended use, with period, interval, variables and values as columns.

period	interval	variable	values
1	hf	abp_power	6.25
1	hf	cbfv_power	3.22
...
2	vlf	gain_norm	1.85
2	vlf	phase	9.38

output = 'plot':

Plot format output table which can be used to draw figures with gain, phase and coherence depending on frequency.

period	freq	gain	phase	coherence
1	0.00	0.16	0.00	0.04

1	0.01	0.29	4.22	0.29
...
2	1.55	1.15	-43.2	0.64
2	1.56	1.16	-41.1	0.42

TFA-parameters

A series of parameters that control TFA analysis (window-length, frequency bands ...). If this is not provided, default values, corresponding to those recommended in the white paper, will be used. These default values are given below for each parameter.

- `vlf` Limits of *very low frequency* band (in Hz). This corresponds to the mathematical inclusion of $[X:Y[$. Default is `c(0.02-0.07)`.
- `lf` Limits of *low frequency* band (in Hz). This corresponds to the mathematical inclusion of $[X:Y[$. Default is `c(0.07-0.2)`.
- `hf` Limits of *high frequency* band (in Hz). This corresponds to the mathematical inclusion of $[X:Y[$. Default is `c(0.2-0.5)`.
- `detrend` Linear detrending of data prior to TFA-analysis (detrending is carried out as one continuous trend over the whole length of the recording, not segment-by-segment). Default is FALSE.
- `spectral_smoothing` The length, in samples, of the triangular spectral smoothing function. Note that this must be an odd number, to ensure that smoothing is symmetrical around the centre frequency. Default is 3.
- `coherence2_thresholds` The critical values (alpha=5%, second column) for coherence for a number of windows (first column, here from 3 to 15). These values were obtained by Monte Carlo simulation, using the default parameter settings for the TFA-analysis (Hanning window, overlap of 50% and 3-point spectral smoothing was assumed). These values should be recalculated for different settings. Note that if `overlap_adjust=TRUE`, the overlap will vary depending on the length of data. With an overlap of 60% (see below), the critical values increase by between 0.04 (for 3 windows) and 0.02 (for 15 windows). Default is `cbind(c(3:15), c(0.51, 0.40, 0.34, 0.29, 0.25, 0.22, 0.20, 0.18, 0.17, 0.15, 0.14, 0.13, 0.12))`.
- `apply_coherence2_threshold` Apply the thresholds given above to the TFA-estimates. All frequencies with magnitude-squared coherence below the threshold value are excluded from averaging when calculating the mean values of gain and phase across the bands. Note that low values of coherence are not excluded in the average of coherence across the bands. Default is TRUE.
- `remove_negative_phase` Remove (ignore) negative values of phase in averaging across bands. Negative phase values are removed only for frequencies below the frequency given below, when calculating the average phase in bands. Default is TRUE.
- `remove_negative_phase_f_cutoff` The cut-off frequency below-which negative phase values are neglected (only if `remove_negative_phase` is TRUE). Default is 0.1.
- `normalize_ABP` Normalize ABP by dividing by the mean and multiplying by 100, to express ABP change in %. Note that mean-values are always removed from ABP prior to analysis. Default is FALSE.

- `normalize_CBFV` Normalize CBFV by dividing by the mean and multiplying by 100, to express CBFV change in %. Note that the band-average values of gain are always calculated both with and without normalization of CBFV, in accordance with the recommendations. Note also that mean-values are always removed from CBFV prior to analysis. Default is FALSE.
- `window_type` Chose window 'hanning' or 'boxcar'. Default is 'hanning'.
- `window_length` Length of the data-window, in seconds. Default is 102.4.
- `overlap` Overlap of the windows, in %. If `overlap_adjust` is TRUE (see below), then this value may be automatically reduced, to ensure that windows cover the full length of data. Default is 59.99% rather than 60%, so that with data corresponding to 5 windows of 100 s at an overlap of 50%, 5 windows are indeed chosen.
- `overlap_adjust` Ensure that the full length of data is used (i.e. the last window finishes as near as possible to the end of the recording), by adjusting the overlap up to a maximum value given by `params.overlap`. Default is TRUE.
- `na_as_mean` Changes all missing non-interpolated values to the mean value of the corresponding variable. This have not been adressed in the paper by Claassen, and to ensure the dataframes are not 'gathered' this should generate the most stable results. Default is TRUE.

References

1. Claassen et al. (2016) J Cereb Blood Flow Metab. 2016 Apr;36(4):665-80. ([PubMed](#))

Examples

```
data(tfa_sample_data)
TFA(tfa_sample_data[,c(1:3)], variables=c("abp", "mcav"), freq=10)
```

tfa_sample_data	<i>TFA sample data</i>
-----------------	------------------------

Description

Dataframe with data provided by Prof. Simpsons, with time (t), arterial blood pressure (abp), left MCAv (mcav_l), right MCAv (mcav_r), and end-tidal CO2 (etco2).

Usage

```
data(tfa_sample_data)
```

Format

An object of class "dataframe"; an example of the usage in [TFA](#)-function.

Source

[GitHub](#)

References

- Simpsons D (2015) ([Cerebral Autoregulation Research Network](#))
- Claassen et al. (2016) J Cereb Blood Flow Metab. 2016 Apr;36(4):665-80. ([PubMed](#))

Examples

```
data(tfa_sample_data)
TFA(tfa_sample_data[,c(1:3)], variables=c("abp","mcav"), freq=10)
```

tfa_sample_data_1	<i>TFA sample data - 1</i>
-------------------	----------------------------

Description

Dataframe with data provided by Prof. Simpsons, with time (t), arterial blood pressure (abp), left MCAv (mcav_l), right MCAv (mcav_r), and end-tidal CO2 (etco2).

Usage

```
data(tfa_sample_data)
```

Format

An object of class "dataframe"; an example of the usage in [TFA](#)-function.

Source

[GitHub](#)

References

- Simpsons D (2015) ([Cerebral Autoregulation Research Network](#))
- Claassen et al. (2016) J Cereb Blood Flow Metab. 2016 Apr;36(4):665-80. ([PubMed](#))

Examples

```
data(tfa_sample_data)
TFA(tfa_sample_data_1[,c(1:3)], variables=c("abp","mcav"), freq=10)
```

tfa_sample_data_2 *TFA sample data - 2*

Description

Dataframe with data provided by Prof. Simpsons, with time (t), arterial blood pressure (abp), left MCAv (mcav_l), right MCAv (mcav_r), and end-tidal CO2 (etco2).

Usage

```
data(tfa_sample_data)
```

Format

An object of class "dataframe"; an example of the usage in [TFA](#)-function.

Source

[GitHub](#)

References

- Simpsons D (2015) ([Cerebral Autoregulation Research Network](#))
- Claassen et al. (2016) J Cereb Blood Flow Metab. 2016 Apr;36(4):665-80. ([PubMed](#))

Examples

```
data(tfa_sample_data)
TFA(tfa_sample_data_2[,c(1:3)], variables=c("abp", "mcav"), freq=10)
```

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